

NANOSPONGE AS A NEW NANOENGINEERING HORIZON FOR DRUG DELIVERY: A REVIEW

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Abstract

Nanosponges are exceptionally permeable, 3D organized, minor size, nanometric cavity size nanocarrier having remarkable capacity to entangle dynamic drug moieties. Nanosponge giving novel drug delivery just as upgrading solubility and bioavailability. The fundamental spotlight is given on cyclodextrin polymer nanostructured inside a 3D network. Indeed, even the cyclodextrin structure edifices with different sort of lipophobic/hydrophobic drug molecules. The incorporated molecules release be fluctuated by modifying structure to acquire quickly and drag out drug molecule release just as at explicit target site. Cyclodextrin nanosponge pull in extraordinary consideration for fathoming issue of bioavailability, deficient solubility, poor disintegration rate, pharmacokinetic issue of different medicaments and expanding drugs productiveness and decreasing superfluous antagonistic impact. It prompts a novel drug delivery framework.

Keywords : Cyclodextrins, Nanosponges, Cross linking agent, Biocompatible.

INTRODUCTION

Nanosponges are tiny mesh-like structures in which different substance can be encapsulated¹⁻². These particles are capable of carrying both lipophilic and hydrophilic substances and of improving the solubility of poorly water suitable molecules²⁻³. The nanosponge is about the size of a virus with a 'backbone' (a scaffold structure) of naturally degradable polyester also a 3D structure¹². The long length polyester strands are mixed in the solution with small molecules called as cross-linkers that have an affinity for certain portions of the polyester. They 'cross link' segments of the polyester to form a spherical shape that has many pockets (or cavities) where drugs can be stored³. These chemical cross linkers enable nanosponge to get bind at preferentially to the target site³⁻⁴. Predictable release is one of major advantage of this system compared to other nanoparticle

delivery system⁵. These nanosponges represent a novel class of nanoparticles usually obtained by the natural derivatives. As compared to the other nanoparticles, they are insoluble in both water and organic solvents, porous, non-toxic and stable at high temperatures up to 300°C. It has been reported that, by reacting cyclodextrins (cyclic oligosaccharides) with suitable cross-linking reagents, a novel nanostructured material consisting of hyper-cross-linked cyclodextrins can be obtained, known as nanosponges¹. Cyclodextrins are cyclic oligomers of D-glucopyranose units linked by (α-1, 4) linkages. A cyclodextrin has a characteristic structure with primary hydroxyl groups extending from the narrow edge and secondary hydroxyl groups extending from the wider edge which impart to cyclodextrins their peculiar hydrophilic outer surface and a lipophilic cavity⁵.

This review includes an emerging approach to prepare multifunctional cyclodextrin derivatives by bringing about crosslinking of cyclodextrin polymers. Cyclodextrin-based nanosponges are a promising and an innovative form of a drug delivery system which comprises a nanostructured three-dimensional network of crosslinked cyclodextrin molecules with a porous structure capable of encapsulating hydrophilic as well as hydrophobic drug molecules⁵⁻⁶. The main common cyclodextrins in these delivery systems are α, β and γ, with 6, 7 and 8 glucopyranose units. Among these, β-CD is mainly selected in the nanosponge preparation, because it is the cheapest and most useful one, with its higher dimension of inner cavity⁶. Cyclodextrin-based Nanosponge CDNSs are known to be non-allergic and biodegradable⁶. Most of the CDNS formulations have high zeta potential value (more than -20 mV) which makes stable nanosuspension in water with little tendency to aggregate longer time. This characteristic of CDNSs can improve the aqueous solubility of poorly water-soluble molecules and overcome major barrier in the delivery of lipophilic drugs in physiological media⁶.

Boons of the Nanosponge

- It is Targeted site specific drug delivery.
- May be used to mask unpleasant flavours and to convert liquid substances to solids [10].
- Less harmful side effects (since smaller quantities of the drug have contact with healthy tissue).
- Nanosponge particles are soluble in water, so the hydrophobic drugs can be encapsulated within the nanosponge,
- Particles can be made smaller or larger by varying the proportion of cross-linker to the polymer.
- The drug profiles can be varied from fast, medium to slow release, preventing over or under-dosing of the therapy .
- Improved stability, increased elegance and enhanced formulation flexibility.
- Nanosponges systems are non-irritating, non-mutagenic, non-allergenic and non-toxic.
- These are self-sterilizing as their average pore size is 0.25 μm, where bacteria will not be able to penetrate .
- Extended release - continuous action up to 12 h.

- It is Biodegradable and Biocompatible⁵⁸.

CDNSs are biocompatible, nontoxic and safe for use. The drug release from these nanosponges can be customized by tuning the type and degree of crosslinking. It possess numerous advantages ranging from improved solubility, stability, permeation, bioavailability, modulation of drug release to efficient drug targeting in case of anticancer therapeutics. In addition, delivery of proteins, enzymes and gases is possible. This system offer many advantages and various applications. The natural CDs with their characteristics are mention in Table 1.

Table 1 - Types of natural CDs and their characteristics^{56,57,41}

Properties	Alpha-CDs	Beta-CDs	Gamma-CDs
The no. of units of glucose	6	7	8
Dimensions (nm)			
Height	0.78	0.78	0.78
Outer diameter	1.37	1.53	1.69
Inner diameter	0.57	0.78	0.95
The Molecular weight	972	1135	1297
The size of cavity	174	262	472
The solubility of water	14.5	1.85	23.2
Applications	Oral, Parental, Topical	Oral, topical	Oral, Parental, Topical

Drug release Mechanism from the Nanosponges

Nanosponge has open structure which provides free movement of drug substance entrapped in vehicle in the outward and inward direction from the nanosponge till the equilibrium reached. Whereas in case of gels or cream, the equilibrium will get disturb because drug itself is in vehicle and tend to become unsaturated. The drug will flow from the nanosponge to the vehicle and further into the skin until and unless the vehicle is absorb or dried. The nanosponge retained on surface layer of skin that is stratum corneum will further release the drug to the skin leading to the prolong release of drug over the certain time⁵⁸ as shown in fig. 5.

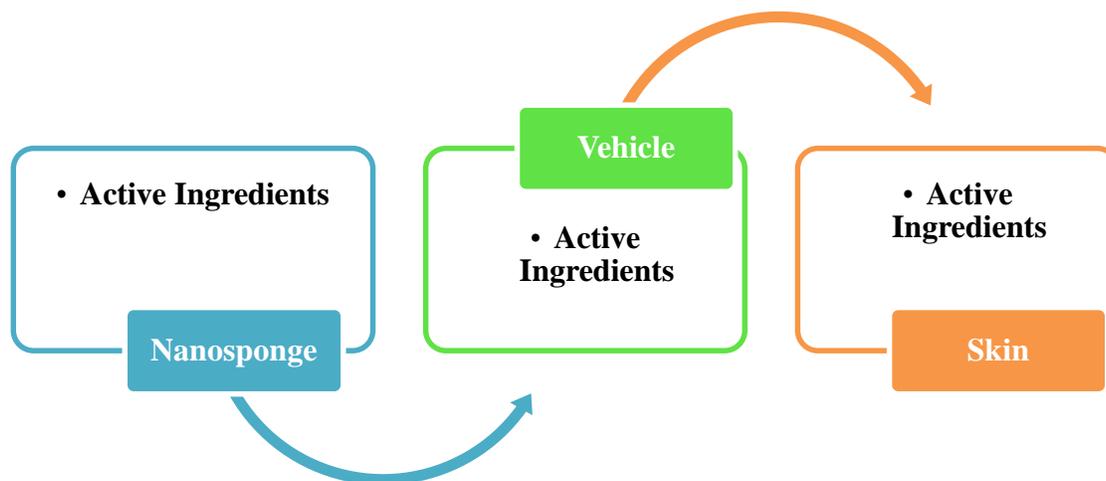


Fig. 5- Mechanism of drug release

APPLICATION OF NANOSPONGES

In Anticancer therapy

Paclitaxel is the drug used for treating cancer related to lungs and ovary. Amphiphilic was developed as a carrier system in the form of the nanoparticle which will encapsulate paclitaxel. Due to this encapsulation the resultant effect is an increase in solubility and loading capacity further forming inclusion complex. The extended release was found to be 24 hr for the nanocapsule and 12 hr for the nanosponge⁸.

Paclitaxel has poor dissolution and water solubility. Hence, to overcome this the β -CD based nanosponges are formulated for paclitaxel. The effect of the drug is enhanced by formulating it in the form of the nanospongedrug intracellular concentrations increase as compared to plain drug¹⁵.

In Gene therapy

Gene therapy has enormous promise for the treatment of an extensive variety of clinical situations. Cyclodextrins have great affinity toward nucleic acids and ability to attenuate the other gene carriers for attenuation¹⁰⁻¹¹. The main reasons for incorporating CDs is to minimize the cytotoxicity by offering a cellular uptake of the nanosponge loaded with the drug⁸. Further this will offer the good delivery of the nucleic acids, DNA and greater amount of protein expression in the mucosa of the respiratory system¹³.

In drug delivery

Nanosponges are nanometric in size and have a spherical shape, therefore, nanosponges can be prepared in different dosage forms like topical, parenteral, aerosol, tablets and capsules¹. Telmisartan (TEL) is a BCS Class II drug having the dissolution rate limited bioavailability. β -CD based nanosponges were formed by the cross-linking β -CD with carbonate bonds. TEL was formulated into the nanosponges. Saturation solubility and in vitro dissolution study of β -CD complex of TEL was compared with the plain drug TEL and nanosponge

complexes of TEL. It was found that solubility of TEL was increased by 8.53 fold in distilled water, 3.35-fold in 1 mol HCl and 4.66 fold in phosphate buffer pH 6.8 by incorporating NaHCO_3 in drug-nanosponges complex than TEL. The highest solubility and in vitro drug release was observed in inclusion complex prepared from nanosponges and NaHCO_3 ^{1,13,14}.

In Sustained delivery system

Acyclovir is majorly used as a antiviral agent in the treatment of the herpes simplex virusinfections¹⁶. Acyclovir has low absorption through the gastrointestinal tract and its incomplete with varying its pharmacokinetic properties when taken orally. The nanosponge formulation of acyclovir has shown the sustained release of the drug. Hence, nanosponge formulation has of acyclovir has overcome the pharmacokinetic issue of the drug. Therelease of acyclovir from Carb-nanospongeswas 70%, respectively¹⁷.

Nanosponge for protein delivery

Proteins are with one of the major issue is the long term stability issue^{1,18}. Proteins get reversibly denature upon lyophilization. Thus, a major problem in protein formulation process is the maintaining the structure of protein during the formulation process as well as for the long term stability¹⁹.

The new swellable cyclodextrinbasedpoly (amidoamine) nanosponges named nanosponges 10 and nanosponges 11, were synthesised by the crosslinking β -CDs with either 2,2-bis-acrylamidoacetic acid or polyamido-amine chain deriving from 2,2-bis-acrylamidoacetic acid and 2-methylpiperazine respectively. The formulated β -CD based poly(amidoamine)-nanosponges were found to be stable at 300 °C and high protein complexation capacity was observed and overcome stability issue of protein²⁰.

Nanosponge in the enzyme immobilization

The problem of the enzyme immobilization is particularly relevant for the lipases, as it modulates properties like enantio selectivity and reaction rates²¹.

The synthesis of Platinum- Silver graphite-nanofiber-supported porous nanosponges and mesoporous platinum nanosponges as electrocatalysts for the purpose of oxygen reduction reaction^{22,23}.

Nanosponges as protective agent from light or degradation

Gamma-oryzanol is the ferulic acid ester mixture, majorly used as a antioxidant of natural source and widely used for stabilizing pharmaceutical raw materials, food, even used as a sunscreen in the cosmetics industry, it is with huge applicability. Photodegradation and instability are its major limitations. Gamma-oryzanol has been protected from photodegradation by encapsulating in nanosponges. Even this nanosponge were also formulated as emulsions and gel²⁵.

Nanosponges in solubility enhancement

The formulation of itraconazole in Nanosponges was done²⁷. Itraconazole drug having poor solubility, dissolution and bioavailability, which is BCS class II drug hence nanosponge approach was chosen. Nanosponges have successfully improved solubility of the itraconazole by greater than 27 folds. Further when the supporting component was added in the above formulation the solubility increase by greater than 55 folds. Mechanism involves in enhancing solubility of drug by nanosponge is by increasing wetting ability of drug and masking the various lipophilic groups in itraconazole as well as by decreasing crystallinity of the drug²⁷. Hence, enhancing solubility of poor water soluble drugs.

For Oral delivery systems

For solid drug the major limiting factor is its dissolution, as per oral bioavailability is concern. The dissolution process acts as the rate-controlling step for the hydrophobic drugs and, hence degree of absorption can be determined. Many hydrophobic drugs have incomplete absorption from the gastrointestinal tract. Acetylsalicylic acid (ASA), one of the BCS Class III drug having NSAIDs (nonsteroidal anti-inflammatory) activity was formulated for its prolonged release with into pyromellitic dianhydride and then cross-linked with β -cyclodextrin nanosponges. The release data of in nanosponge was obtained by *in vivo* and *in vitro* studies. Shown the delayed release of drug over a prolonged period of the 24 hr. These obtained results indicate that many drugs with poor water solubility can be used for oral delivery for formulating the particular drug in nanosponge formulation²⁸.

Topical delivery systems

For topical application the nanosponge can be used in form of creams, gels etc. Resveratrol, a herbal molecule which is important to treat various human diseases and due to its antioxidant properties but has poor solubility and stability, hence it was formulated in nanosponge which has enhanced its solubility and stability. Resveratrol-loaded nanosponges have not only increased solubility but also its permeation in *in vitro* studies using porcine skin⁷.

Patents in the field of cyclodextrin based nanosponges are given in Table 2.

Table 2: Patents of cyclodextrin based nanosponges

Title	Publication Number	Publication Date
Preparation of crosslinked cyclodextrin resins with enhanced porosity	US4958015 A [50]	1990
Cyclodextrin polymer and cyclodextrin film	EP0502194 A1 [51]	1992

formed therefrom		
Cross-linked polymers based on cyclodextrins for removing polluting agents	US20050154198A1 [52]	2003
Ultrasound-assisted synthesis of cyclodextrinbased nanosponges	US20080213384A1 [55]	2006
Cyclodextrin nanosponges as a carrier for biocatalysts, and in the delivery and release of enzymes, proteins, vaccines and antibodies	EP2294190A1 [54]	2010
Cyclodextrin-based nanosponges as a vehicle for antitumoral drugs	EP2175847A1 [53]	2011

Method of synthesis of Nanosponges

Emulsion solvent diffusion method

The nanosponges were prepared with Ethyl cellulose and Polyvinyl alcohol in variable ratios. This method having two phases that are continuous phase and dispersed phase. The dispersed phase having ethyl cellulose and drug were added in dichloromethane (20 ml) and gently mixed in a continuous phase which containing exact quantity of PVA in water (150 ml). The solution was stirred continuously for 2hrs. at 1000 rpm. After stirring is over, by using vacuum filtration formed nanosponges were collected. After filtration the nanosponges were dried for 24 hrs at 40°C in an oven and for the withdraw of residual solvent it was stored in a vacuum desiccator⁴ as shown in fig. 2.

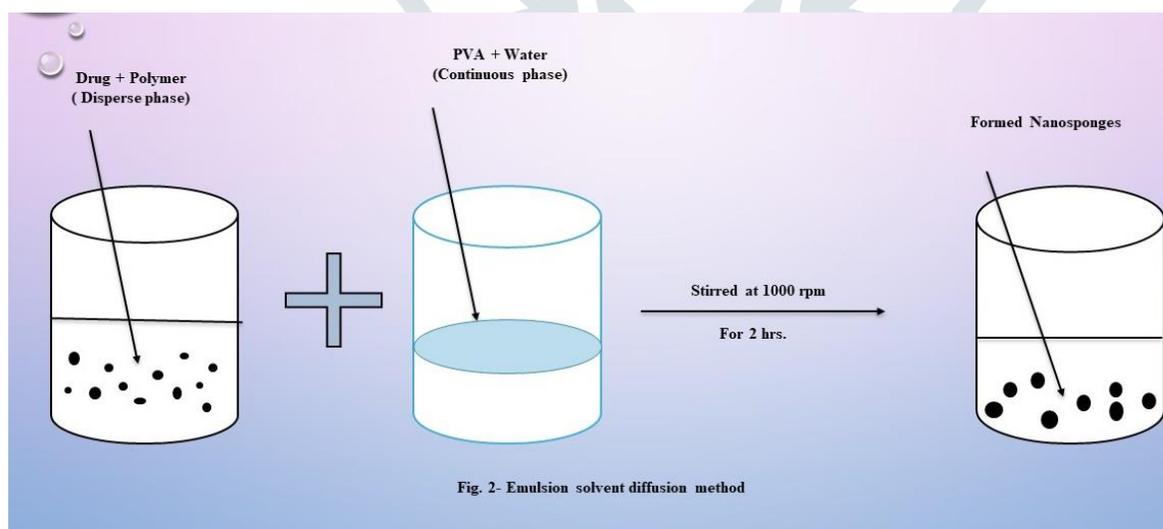


Fig.2. Emulsion solvent diffusion method

Formulation of nanosponges by Hyper-crosslinked β -CDs

The various types of CDs with carbonate compounds as a crosslinking agent can be used to prepare nanosponges. In round bottomed flask added 100 ml of dimethylformamide and 17.42 g of anhydrous β -CD for complete dissolution. Then carbonyl diimidazole (9.96 g) was added and the solution was reacted at 100°C for 4 hrs. After completion of condensation polymerization, the hyper-crosslinked CDs were broken roughly and to withdraw dimethylformamide excess amount of deionized water was mixed. At last Soxhlet extraction was used with ethanol to withdraw the unwanted reagents. The achieved β -CDs nanosponges were dried in oven at 60°C for overnight and later broken into mortar. In water the obtained nanosponges were added. The retained colloidal part in water was collected and lyophilized. Hyper-crosslinked β -CDs nanosponges were obtained with spherical shape and submicron in dimension⁴ as shown in fig. 1.

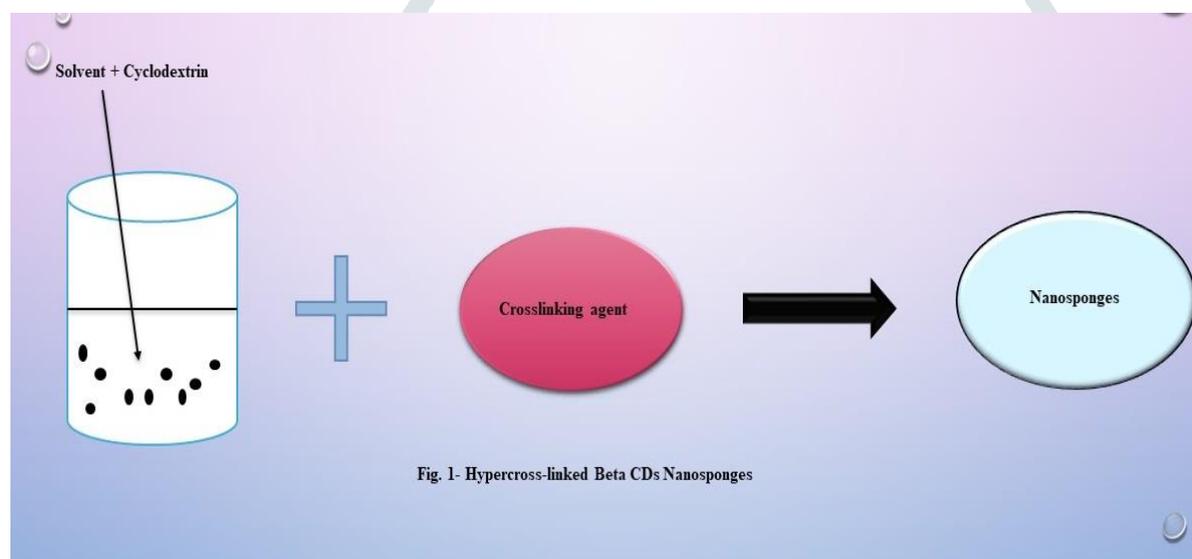


Fig.1- Hypercross-linked Beta CDs Nanosponges

Solvent Method

solvent method, a polymer was added in a suitable solvent like Dimethylformamide and Dimethylsulfoxide as shown in fig. 3. Then excess amount of crosslinker was added in that mixture. Molar ratio of crosslinker/polymer preferably in 4:16. Temperature of reaction mixture was increasing at 10°C to solvent reflux temperature for 1-48 hrs. After reaction completed, at room temperature the mixture was cooled. In excess bidistilled water the formed nanosponges were mixed. Then recovered the formed nanosponges with filtration. At last the Soxhlet extraction was used with ethanol to withdraw unreacted reagents. Preferred crosslinkers are Dimethyl carbonate and carbonyl diimidazole¹ as shown in fig 3.

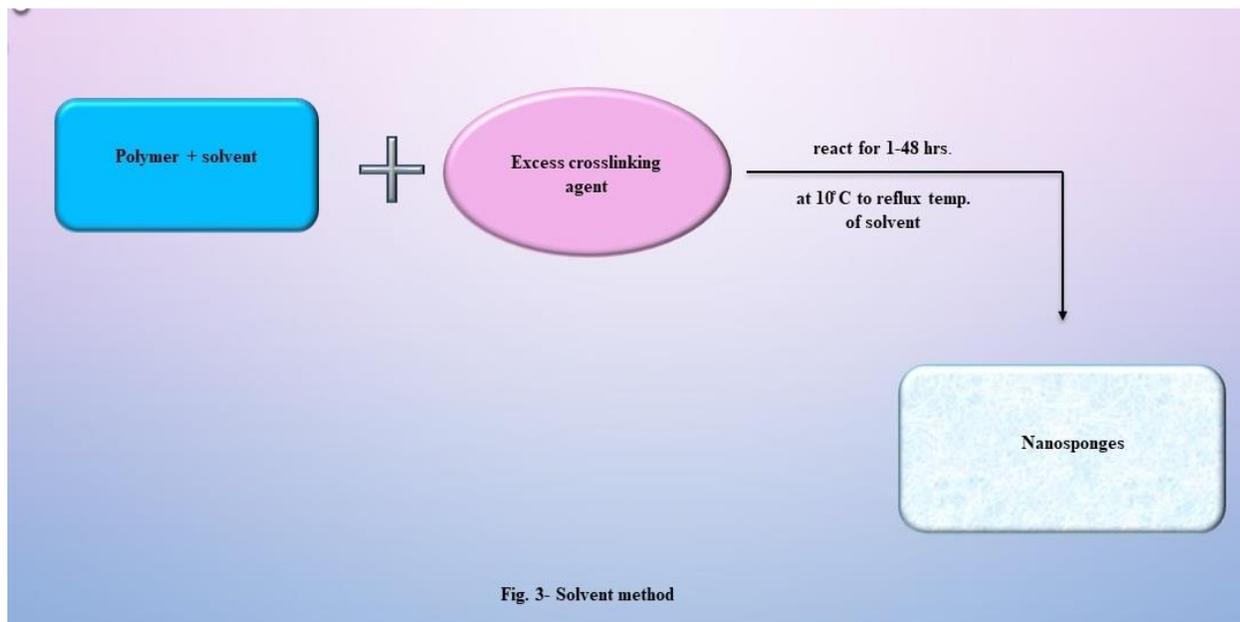


Fig.3. Solvent Method

Ultrasound-assisted synthesis

The nanosponges were achieved by reaction of crosslinking agent and polymers. In this method solvents are not used. In a suitable ratio the polymer and crosslinking agent were mixed into flask. On a ultrasound bath the flask was kept and sonicate the mixture for 5hrs. at a 90°C temperature. Then at a room temperature the solution was cooled and roughly broken the obtained nanosponges. To withdraw the unreacted reagents the obtained nanosponges were washed with distilled water. At last the Soxhlet extraction was used with ethanol for purification of nanosponges. The obtained nanosponges were dried and for further purpose it was stored at 25°C. The obtained nanosponges were uniform and spherical in shape³ as shown in fig 4.

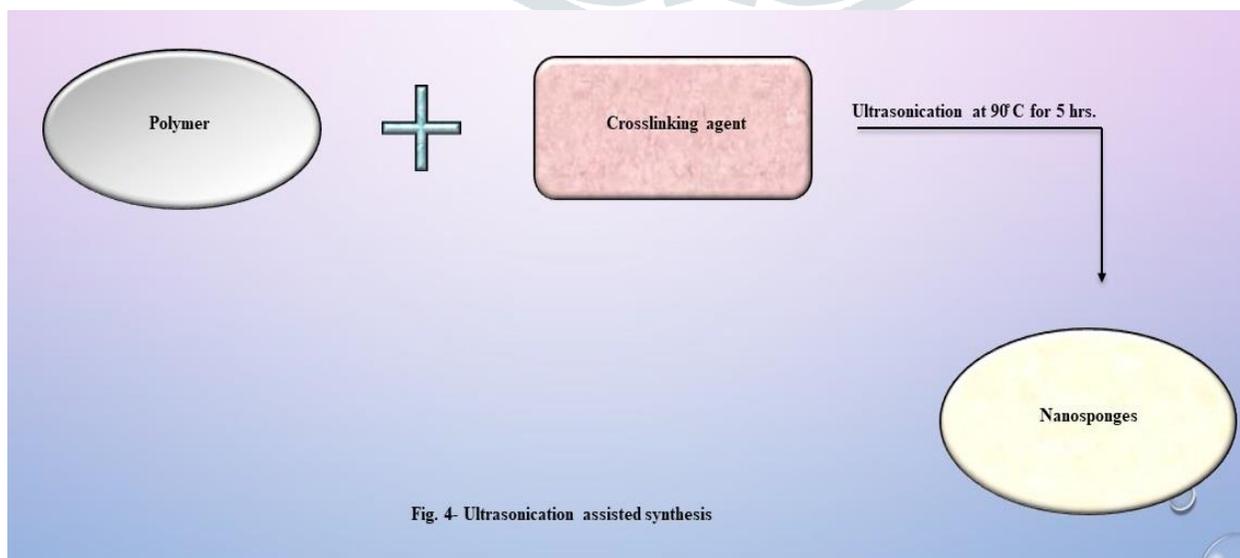


Fig.4- Ultrasound assisted synthesis

Loading of drug into nanosponges

To achieve the average particle size below 500nm the nanosponges for delivery of drug should be pretreated. In water the obtained nanosponges were suspended and to remove the aggregation of particles the solution was sonicated and to achieve the colloidal fraction the solution was centrifuged. After centrifugation of suspension separate the supernatant and by using lyophilization/freeze drying sample was dried. Nanosponge suspension was formulated and mixed excess quantity of drug into suspension. After addition of drug, it kept for continuous stirring for a particular time. After completion of stirring, by centrifugation the unreacted drug was removed. The nanosponges can be achieved by lyophilization/freeze drying. The structure of nanosponges are very important. The loading of drug into nanosponges are better in crystalline nanosponges compared to paracrystallinenanosponges¹.

Factors affecting nanosponges formulation

Type of polymers

The polymers which are using in the preparation of the nanosponges may be affect the performance and formation of the nanosponges. The cavity of nanosponges should have appropriate size where drug can fit easily³.

Few examples polymers, cross-linkers and solvent are shown in Table 3.

Table 3- Examples of polymer, solvent and cross- linkers

Polymers	EthylCellulose and PVA, Eudragit RS 100, Copolymers like Poly (valerolactone -allylvalerolactone), Hyper crosslinked Polystyrenes, Cyclodextrins and its derivatives like Methyl β - Cyclodextrin, 2-Hydroxy Propyl β -Cyclodextrins.
Cross-linkers	Dichloromethane, Carbonyl Diimidazole, Diphenyl Carbonate, Di-Isocyanates, Pyromellitic anhydrid, Diarylcarbonates, Glutaraldehyde, Carboxylic acid dianhydrides.
Solvents	Dimethylacetamide, Dimethyl Sulfoxide, Ethanol, Dimethylformamide.

Type of Drugs

The drug molecule compounded with nanosponges should have following ideal properties:

1. The molar mass of drug substance should be between 100-400 Dalton.

2. The drug substance should not have more than five condensed rings.
3. The solubility of drug substance should not be more than 10 mg/ml.
4. The melting point should not be above 250°C⁴.

Examples of drug used for cyclodextrin based nanosponge are given in Table 4.

Table 4- Drugs used for cyclodextrin based nanosponge

Drug	Nanosponge vehicle	Indication	Reference
Paclitaxel	β-Cyclodextrin	Cancer	44,45
Camptothecin	β-Cyclodextrin	Cancer	35,46
Tamoxifen	β-Cyclodextrin	Breast cancer	43
Resveratrol	β-Cyclodextrins	Cardiovascular disease, Inflammation	47
Itraconazole	β-Cyclodextrin&Copolyvidonum	Antifungal	48
Dexamethasone	β-Cyclodextrin	Brain tumors	49

Temperature

The changes in temp can affect the Drug/Nanosponges complexation. The increase in the temperature decreases the magnitude of the apparent stability constant of the Drug/Nanosponge complex may be due to the result of possible reduction of the drug/nanosponge interaction forces, such as Hydrophobic forces and Van- Der Waals forces with increase in the temperature

Method of preparation

The method for the loading of the drug into nanosponge can affect the Drug/Nanosponge complexation. The effectiveness of the method depends on the nature of the drug and polymer. In most of the cases Freeze drying was found to be most effective for drug complexation.

Degree of substitution

The type, number, and position of substituent of the parent molecule can be highly influence the compounding capacity of nanosponges³.

CHARACTERIZATION OF NANOSPONGE

Particle size and polydispersity Index

Particle Size Analyser Nanoplus a particle sizing software is majorily used for determining the particle size by using dynamic light scattering. This will provide data of the mean diameter through which the polydispersity index would be able to identify of the nanosponge^{31,32,2}. PDI is an index of the width or variation within the particle size distribution of the given sample. Generally higher the value of PDI wider the particle size distribution and monodisperse sample generally possed lower PDI value. . PDI could be calculated by the following equation:

$$PDI = \Delta d / d_{avg}$$

Where,

Δd is the width of distribution denoted as SD and d_{avg} is the average particle size denoted as MV (nm) in particle size data sheet³³. Refrence value are given in Table 5

Table 5- PDI

Type of dispersion	PDI
Monodisperse standard	0-0.05
Nearly monodisperse	0.05-0.08
Midrange polydispersity	0.08-0.7
Very polydisperse	0.7

Zeta potential

Zeta potential is the measure of surface charge. It can be measured by using additional electrode in the particle size equipment³³.

Infra red spectroscopy

Infra-red spectroscopy is used to estimate the interaction between drugs molecule in solid state and nanosponges. Nanosponges bands often change only slightly upon complex formation. If the fraction of the guest molecules encapsulated in the complex is less than 25%, The technique is not generally suitable to detect the inclusion complexes and is less clarifying than other methods²⁵.

Powdered X ray diffractometry

Powder x-beam diffractometry is used to recognize consideration complex in strong states as well as crystallinity. If fluid is considered, at that point it has no diffraction example of their own and absolutely varies from in complexed nanosponge. On the off chance that tranquilize is a strong substance examination ought to be made between diffractogram of accepted mind boggling and mechanical blend of dry and it adjusts diffraction

patterns. A diffraction example of a physical blend results from mix of two parts. Be that as it may, edifices having diffraction design for the most part contrasts from the constituent they contain and offer ascent to "new" strong stage having diverse diffractograms. They offer ascent to various crests for a blend and valuable in deciding concoction decay and complex development²⁹.

Entrapment Efficiency

Nanosponge entrapment efficiency can be determined by quantitative estimation of the drug loaded into nanosponges by the UV spectrophotometer and high performance liquid chromatography methods. The entrapment efficiency (%) of nanosponges can be calculated according to the following equation⁴.

$$\text{Entrapment Efficiency} = \frac{\text{calculated drug content in nanosponge}}{\text{Theoretical drug content}} \times 100$$

Microscopy studies

Scanning Electron Microscopy (SEM) and Transmission Electron Microscopy (TEM) are used to study the microscopic aspects regarding size of drugs nanosponges as well as cavities present and drug loaded into cavities (drug/nanosponge complex)^{34,35}.

Thermo-analytical methods

Thermo-analytical methods is for determining whether drug is compatible with the other ingredients used or drug substance undergoes few change regarding endo and exothermic peak before the thermal degradation of nanosponge. Melting, decomposition, oxidation or polymorphic transition which gives idea about change in the drug substance. Obtained thermogram by DSC and DTA were observed for the shifting, broadening and appearance of new peaks or disappearance of particular peaks. Mostly changes in weight loss also provide indication for the formation of inclusion complexes³⁸.

Phase Solubility study

Phase solubility method is one of the majorly used method for studying inclusion complexation described by Higuchi and Connors, providing the effect of formulated nanosponge on the solubility of drug^{39,40,41}. In this method the drug in nanosponge form was added to a shaking flask incubator containing an aqueous solution of various percentages of nanosponges. The Shaking flask incubator's temperature and required rpm speed was maintained. After completion of given time the suspension was taken out and centrifugation was done using a molecular filter of 3 000 Dalton. The supernatant solution obtained was further analyzed to determine the drug concentration by UV visible spectroscopy method.

In-vitro study of drug release

Franz Diffusion cell is commonly used by using dialysis membrane for studying drug release of formulated nanospongewith diffusional area of 2.26 cm² and 11 ml of receptor volume. The dialysis membraneto be used must be soaked for 8 hr in the medium to be used and this membrane will act as barrier between receptor and donor compartment. Then the nanosponge of 1 g was placed on donor chamber which was further seal by aluminum foil from the atmosphere. Compartment receptor was further filled with the 6.8 pH phosphate buffer of by the volume of 11 ml. During the experiment, the temperature and speed was maintained that is the 37±0.5°C and at 100 rpm of stirring, solution of receptor side compartment was further kept at Teflon-coated magnetic stirring bars. As per the reported time intervals the aliquot was collected from the receptor chamber and replaced by same volume of the media for maintain sink condition. Further sample was analyzed for drug release using UV visible spectrophotometer⁴².

CONCLUSION

The nanosponges are novel class of drug delivery system and it consist of three-dimensional network. The nanosponge structure consist of cavities on their surface where drug molecule can be incorporated. The nanosponges are biocompatible with various types of drug molecule and due to which they are non-toxic, non-irritant and non-allergenic. The nanosponges have good ability to incorporate lipophilic/hydrophilic drug molecules. The nanosponges can be prepared into the different dosage forms such as parenteral, topical, capsules, aerosols and tablets. The nanosponges not only having the ability to solve the solubility problem of drug but also enhance the permeation, prolonging release of drug substance, stability and bioavailability. The cyclodextrin based nanosponges are also used for the delivery of important pharmaceutical gases and proteins. The nanosponges contains wide range of applications in pharmaceutical and medicines as well as in various field like environment, cosmetics and the agriculture. From above study we can conclude that nanosponges have multipurpose use, therefore this system is appropriate for delivery of active ingredient in nanomedicine.

REFERENCES

1. Panda S, Vijayalakshmi S, Pattnaik S, Swain RP. Nanosponges: A novel carrier for targeted drug delivery. **Int J PharmTech Res.** 2015,8(7),213–24.
2. Shringirishi M, Prajapati SK, Mahor A, Alok S, Yadav P, Verma A. Nanosponges: A potential nanocarrier for novel drug delivery-a review, **Asian Pacific J Trop Dis.** 2014,4(S2),S519–26.
3. Subramanian S, Singireddy A, Krishnamoorthy K, Rajappan M. Nanosponges: A novel class of drug delivery system - Review, **J Pharm Pharm Sci.** 2012,15(1),103–11.

4. Bolmal UB, Manvi F V, Rajkumar K, Sowjanya Palla S, Paladugu A, Reddy KR.: Recent Advances in Nanosponges as Drug Delivery System, **Int J Pharm Sci Nanotechnol** . 2013,6(1),34–44.
5. Chilajwar S V., Pednekar PP, Jadhav KR, Gupta GJC, Kadam VJ.: Cyclodextrin-based nanosponges: A propitious platform for enhancing drug delivery, **Expert Opin Drug Deliv**. 2014,11(1),11–20.
6. Allahyari S, Trotta F, Valizadeh H, Jelvehgari M, Zakeri-Milani P.: Cyclodextrin-based nanosponges as promising carriers for active agents,**Expert Opin Drug Deliv** . 2019,16(5),467–79.
7. Trotta F, Zanetti M, Cavalli R.: Cyclodextrin-based nanosponges as drug carriers,. **Beilstein J Org Chem**. 2012,8,2091–9.
8. Lakkakula JR, Maçedo Krause RW.: A vision for cyclodextrin nanoparticles in drug delivery systems and pharmaceutical applications, **Nanomedicine**. 2014,9(6),877–94.
9. Adeoye O, Cabral-Marques H.: Cyclodextrin nanosystems in oral drug delivery: A mini review. **Int J Pharm** . 2017,531(2),521–31.
10. Conceicao J, Adeoye O, Cabral-Marques HM, Lobo JMS. :Cyclodextrins as Drug Carriers in Pharmaceutical Technology: The State of the Art, **Curr Pharm Des**. 2017,24(13),1405–33.
11. Lai WF. Cyclodextrins in non-viral gene delivery, **Biomaterials** .2014, 35(1), 401-11.
12. Vishwakarma A, Nikam P, Mogal R, Talele S: Review on nanosponges: A benefication for noveldrug delivery,**Int J Pharm Tech Res**. 2014,6(1),11-20.
13. Teijeiro-Osorio D, Remuñán-López C, Alonso MJ. :Chitosan/cyclodextrin nanoparticles can efficiently transfect the airway epithelium *in vitro*, **Eur. J. Pharm. Biopharm**.2009, 71(2), 257–263 .
14. Rao M, Bajaj A, Khole I, Munjapara G, Trotta F.: In vitro and in vivo evaluation of β - cyclodextrin-based nanospongesoftelmisartan, **J Incl Phenom Macrocycl Chem**.2013, 77,135-145.
15. Mognetti B, Barberis A, Marino S, Berta G, Francia SD, Trotta F, et al. In vitro enhancement of anticancer activity of paclitaxel by a cremophor free cyclodextrin-based nanosponge formulation. **J Incl Phenom Macrocycl Chem** 2012; 74: 201-210.
16. O'Brien JJ, Campoli-Richards DM. Acyclovir. An updated review of its antiviral activity, pharmacokinetic properties and therapeutic efficacy. **Drugs** 1989; 37: 233-309.

17. Lemboa D, Swaminathan S, Donalisoa M, Civraa A, Pasterod L, Aquilanod D, et al. Encapsulation of acyclovir in new carboxylated cyclodextrin-based nanosponges improves the agent's antiviral efficacy. **Int J Pharm.**2013, 443, 262-272.
18. Klibanov AM, Schefiliti JA. :On the relationship between conformation and stability in solid pharmaceutical protein formulations, **Biotechnol Lett.** 2004, 26,1103-1106.
19. Shewarts D, Sofia S, Friess W.: Integrity and stability studies of precipitated rhBMP-2 microparticles with a focus on ATR-FTIR measurements, **Eur J Pharm Biopharm.**2006,63, 241-248.
20. Swaminathan S, Cavalli R, Trotta F, Ferruti P, RanucciE, Gerges I, et al.: In vitro release modulation and conformational stabilization of a model protein using swellable polyamidoamine nanosponges of β -cyclodextrin, **J Incl Phenom Macrocycl Chem.** 2010, 68, 183-191.
21. Mateo C, Palomo JM, Fernandez-Lorente G, GuisanJM, Fernandez-Lorente R.: Improvement of enzyme activity, stability and selectivity via immobilization techniques., **Enzyme Microb Technol.**2007, 40, 1451-1463.
22. Lee CL, Chao YJ, Chen CH, Chiou HP, Syu CC.: Graphite nanofiber-supported porous Pt-Ag nanosponges: synthesis and oxygen reduction electrocatalysis, **Int J Hydro Energy** 2011, 36,15045-15051.
23. Lee CL, Wu CC, Chiou HP, Syu CM, Huang CH, Yang CC.: Mesoporous platinum nanosponges as electrocatalysts for the oxygen reduction reaction in an acidic electrolyte, **Int J Hydro Energy.**2011, 36, 6433-6440.
24. Mamba BB, Krause RW, Malefetse TJ, Gericke G, Sithole SP.: Water Institute of Southern Africa (WISA) Biennial Conference 2008, Sun City, South Africa, **Special Edition**, 2009, 35(2), 56.
25. Sapino S, Carlotti ME, Cavalli R, Ugazio E, Berlier G, GastaldiL, et al. Photochemical and antioxidant properties of gamma oryzanolin beta-cyclodextrin-based nanosponges, **J Incl Phenom Macrocycl Chem.** 2013, 75,69-76.
26. Cavalli R, Akhter AK, Bisazza A, Giustetto P, Trotta F, VaviaP.: Nanosponge formulations as oxygen delivery systems, **Int J Pharm.**2010,402, 254-257.
27. Swaminathan S, Vavia PR, Trotta F, Torne S.: Formulation of beta cyclodextrin based nanosponges of itraconazole, **J Incl Phenom Macrocycl Chem.** 2007,57(1-4), 89-94.

28. Mognetti, B.Barberis, A.Marino, S.,Berta, G., De Francia, S.,Trotta,Cavalli, R. J.: **Inclusion Phenom. Macrocyclic Chem.** 2012,74, 201–210.
29. Lee CL,Chiou HP, Syu CC.:Graphitenanofiber-supported porous Pt-Ag nanosponges: synthesis and oxygen reduction electrocatalysis. **Int J Hydro Energy** 2011, 36,15045-15051.
30. Alongi, J., Poskovic, M., Frache, A. and Trotta, F., 2011.: Role of β -cyclodextrin nanosponges in polypropylene photooxidation, **Carbohydrate Polymers.** 86(1), 127-135.
31. Renuka S, Kamla P.: Polymeric nanosponges as an alternative carrier for improved retention of econazole nitrate onto the skin through topical hydrogel formulation, **Pharm Dev Technol.** 2011,16(4),367-376.
32. Shankar S, Linda P, Loredana S, Francesco T, Pradeep V, Dino A, Michele T, Gianpaolo Z, Roberta C.: Cyclodextrin-based nanosponges encapsulating camptothecin: Physicochemical characterization, stability and cytotoxicity, **Eur J Pharm Biopharm.** 2010, 74,193-201.
33. Wolfgang S.: Sample preparation in Light Scattering from Polymer Solutions and Nanoparticle Dispersions, **Springer Berlin Heidelberg GmbH & Co.**2007, 43-44
34. Singh R, Bharti N, Madan J, Hiremath SN.: Characterization of cyclodextrin inclusion complexes-a review, **J Pharm Sci Technol.** 2010,2(3),171-183.
35. Shankar S, Linda P, Loredana S, Francesco T,Pradeep V, Dino A, Michele T, GianpaoloZ,Roberta C.: Cyclodextrin-based nanosponges encapsulating camptothecin: Physicochemical characterization, stability and cytotoxicity, **Eur J Pharm Biopharm.**2010, 74, 193-201.
36. Roger AR, valentine JS. Pharmaceutical applications of Cyclodextrins. 2.: In Vivo Drug Delivery, **J.Pharm.Sci.** 1996, 85(11),1142-1169.
37. Patel EK, Oswal RJ.: Nanosponge and microsponges: a novel drug delivery system, **Int J Res Pharm Chem.** 2012, 2(2),237-244.
38. Ramnik S, Nitin B, Jyotsana M, Horemat SN.:Characterization of Cyclodextrin Inclusion complexes –A Review, **J Pharm Sci Tech.**2010,2(3),171-183.

39. Trotta F, Cavalli R, Tumiatti W, Zerbinati O, Rogero C, Vallero R, inventors. Sea Marconi Technologies Sas, assignee.: Ultrasound assisted synthesis of cyclodextrin-based nanosponges, EP 1786841 B1. 2007 June 22.
40. Singh R, Bharti N, Madan J, Hiremath SN.: Characterization of cyclodextrin inclusion complexes-a review, **J Pharm Sci Technol.** 2010, 2(3), 171-183.
41. Challa R, Ahuja A, Ali J, Khar RK.: Cyclodextrins in drug delivery: an update review, **AAPS PharmSciTech.** 2005, 6(2), E329-E357
42. Renuka S and Kamla P.: Polymeric nanosponges as an alternative carrier for improved retention of econazole nitrate onto the skin through topically hydrogel formulation, **PharmDev Technol.** 2011, 367-376.
43. Jenny A, Merima P, Alberto F, Francesco T.: Role of β - cyclodextrin nanosponges in polypropylene photooxidation, **Carbohydrate Polymers.** 2011, 86, 127– 135.
44. Torne SJ, Ansari KA, Vavia PR, Trotta F, Cavalli R.: Enhanced oral Paclitaxel bioavailability after administration of Paclitaxel loaded nanosponge, **Drug Delivery.** 2010, 17(6), 419–425.
45. Ansari KA, Torne SJ, Vavia PR, Trotta F, Cavalli R.: Paclitaxel loaded nanosponges: in-vitro characterization and cytotoxicity study on MCF-7 cell line culture, **Curr Drug Deliv.** 2011, 8(2), 194- 202.
46. Rosalba M, Roberta C, Roberto F, Chiara D, Piergiorgio P, Leigh E, Li S, Roberto P.: Antitumor activity of nanosponge-encapsulated Camptothecin in human prostate tumors. **Cancer Res.** 2011; 71:4431
47. Khalid AA, Pradeep RV, Francesco T, Roberta C.: Cyclodextrin-based nanosponges for delivery of Resveratrol: In Vitro characterisation, stability, cytotoxicity and permeation Study, **AAPS PharmSciTech.** 2011, 12(1), 279-286.
48. Shankar S, Vavia PR, Francesco T, Satyen T.: Formulation of Beta cyclodextrin based nanosponges of Itraconazole, **J Incl Phenom Macrocycl Chem.** 2007, 57, 89–94.
49. Lala R, Thorat A, Gargote C.: Current trends in β -cyclodextrin based drug delivery systems, **Int J Res Ayur Pharm.** 2011, 2(5), 1520-1526.

50. Vitaglione P, Sforza S, Galaverna G, Ghidini C, Caporaso N, Vescovi PP, et al.: Bioavailability of trans-resveratrol from red wine in humans, **Mol Nutr Food Res.** 2005,49(5),495-504.
51. Madaan K, Lather V, Pandita D.: Evaluation of polyamidoamine dendrimers as potential carriers for quercetin, a versatile flavonoid, **Drug Del.** 2016,23(1),254-62.
52. Madhavi BB, Kusum B, Chatanya CK, Madhu MN, Harsha VS, Banji D.: Dissolution enhancement of favirenz by solid dispersion and PEGylation techniques, **Int J Pharm Invest.** 2011,1(1),29.
53. Purvis T, Mattucci ME, Crisp MT, Johnston KP, Williams RO.: Rapidly dissolving repaglinide powders produced by the ultra-rapid freezing process, **AAPS Pharm Sci Tech.** 2007,8(3),E52-E60
54. Gilardi G, Trotta F, Cavalli R, Ferruti P, Ranucci E, Di NG, et al., inventors; Sea Marconi Technologies Sas Di Vander Tumiatti, assignee. Cyclodextrin nanosponges as a carrier for biocatalysts, and in the delivery and release of enzymes, proteins, vaccines and antibodies. European patent EP2294190A1. 2011 Mar 16.
55. Trotta F, Cavalli R, Tumiatti W, Zerbinati O, Roggero C, Vallero R, inventors; Sea Marconi Technologies Di W Tumiatti Sas, assignee.: Ultrasound-assisted synthesis of cyclodextrin-based nanosponges. United States patent US20080213384A1. 2006 Sep 04.
56. Vyas A, Saraf S, Saraf S.: Cyclodextrin based novel drug delivery systems, **J Incl Phenom Macro.** 2008,62(1-2),23-42
57. Tejashri G, Amrita B, Darshana J.: Cyclodextrin based nanosponges for pharmaceutical use: A review, **Acta Pharmaceut.** 2013,63(3),335-58.
58. Osmani Riyaz Ali M, Thirumaleshwar Shailesh, Bhosale Rohit R, Kulkarni Parthasarathi K. Nanosponges: The spanking accession in drug delivery-An updated comprehensive review, **Der Pharm Sin.** 2014,5(6),7-21.
59. Cavalli, R., Rogero, C.M., Mognetti, B., Berta, G.N., Tumiatti, V. and Trotta, F.: Inventors; Sea Marconi Technologies Sas, assignee, Cyclodextrin-based nanosponges as a vehicle for antitumor drugs. **WO.** 2009, 3656, 1.
60. Jilsha, G. and Viswanad, V.: Nanosponges: A novel approach of drug delivery system. **Int J Pharm Sci Rev Res.** 2013,19(2),119-123.